

## 1 Tunable Interpenetrating Polymer Network Hydrogels Based on 2 Dynamic Covalent Bonds and Metal–Ligand Bonds

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Cite This: <https://dx.doi.org/10.1021/acs.macromol.0c00494>



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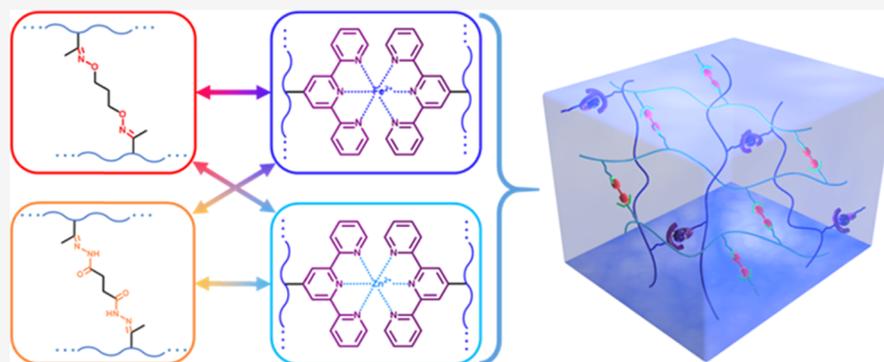
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4 **ABSTRACT:** A series of tunable interpenetrating polymer network (IPN) hydrogels are designed by the orthogonal incorporation  
5 of two distinct types of reversible bonds, i.e., Schiff base bonds and metal–ligand coordination bonds. Two copolymers based on  
6 poly(*N,N*-dimethyl acrylamide) (PDMA) are synthesized and used as building blocks for the IPN hydrogels. The first one bears  
7 ketone pendant groups and is cross-linked by dihydrazide or bishydroxylamine compounds to form, respectively, hydrazine- or  
8 oxime-based dynamic covalent bond (DCB) networks. The second one bears terpyridine side groups and is cross-linked by the  
9 addition of two different transition-metal cations to obtain supramolecular networks based on metal–terpyridine bis-complexes.  
10 Several IPN hydrogels are prepared by combining these different types of reversible bonds to investigate how the two subnetworks  
11 influence each other. To this end, the influence of the cross-linker nature and of the hydrogel preparation protocol on the rheological  
12 properties of these IPNs are also studied in detail. In particular, we show that the obtained IPN hydrogels exhibit a higher modulus  
13 compared to the simple addition of the moduli of the single networks, which we attribute to the entanglements between the two  
14 networks. We then study how these IPN hydrogels can disentangle and partially relax if one of the reversible subnetworks is  
15 composed of cross-links with a shorter lifetime. Finally, pH is used as a stimulus to affect the dynamics of only one of the  
16 subnetworks, and the impact of this change on the properties of the IPNs is investigated.

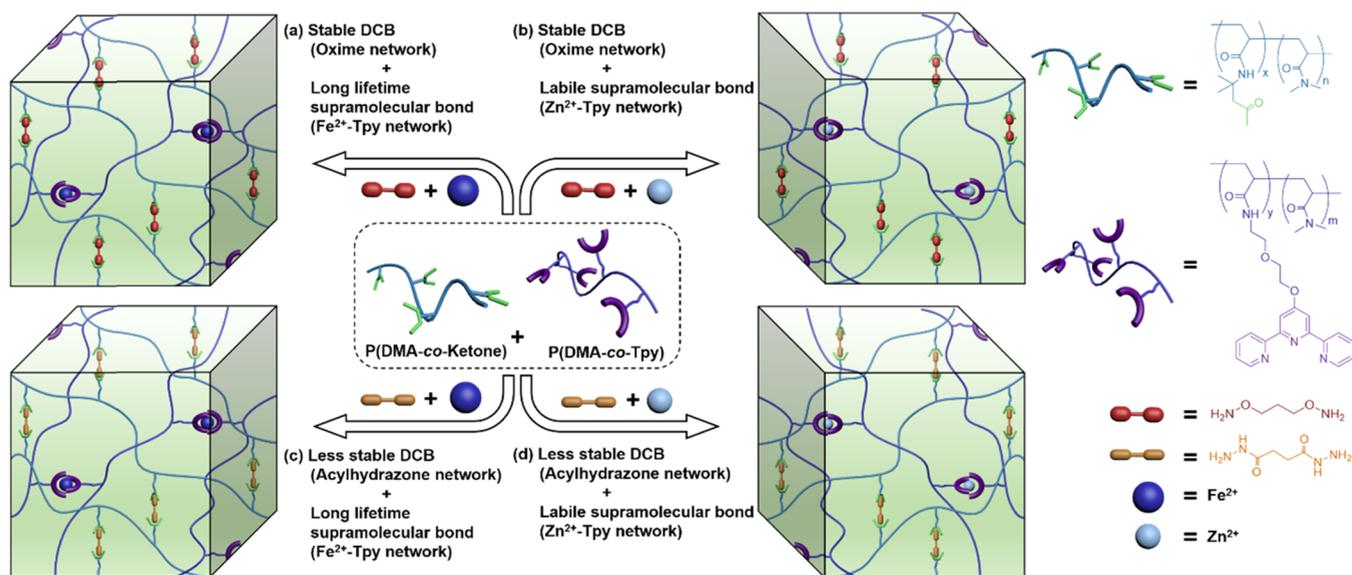
### 17 ■ INTRODUCTION

18 Polymer hydrogels, which are three-dimensional (3D) net-  
19 works composed of cross-linked hydrophilic polymers  
20 entrapping substantial amounts of water,<sup>1</sup> are materials of  
21 choice for multiple applications such as drug delivery,<sup>2</sup> tissue  
22 engineering,<sup>3</sup> 3D printing,<sup>4</sup> wearable devices,<sup>5</sup> actuators,<sup>6</sup>  
23 energy-storage devices,<sup>7</sup> and bioelectronics.<sup>8</sup> To impart further  
24 tunability and adaptiveness to these hydrogels, dynamic or  
25 reversible cross-links are often used to build the networks.<sup>9,10</sup>  
26 These types of linkages encompass dynamic covalent bonds  
27 (DCBs) and supramolecular interactions, both of which can  
28 selectively and autonomously undergo reversible formation,  
29 breaking, and re-formation under equilibrium control.<sup>11</sup> In  
30 general, DCBs such as Schiff base bond (imine, acylhydrazone,  
31 and oxime), Diels–Alder adduct, disulfide bond, boronic ester  
32 bond, etc. have often relatively slow dynamics,<sup>12</sup> while  
33 supramolecular interactions including hydrogen bonding,  
34 metal–ligand complex, host–guest interaction, etc. have faster

dynamics.<sup>13</sup> On account of the peculiar characteristics of DCBs  
35 and supramolecular interactions, the orthogonal combination  
36 of these two categories of cross-links to fabricate networks for  
37 responsive polymer hydrogels or elastomers has received a  
38 rapidly growing attention over the past few years.<sup>14–20</sup>  
39 Compared to networks based on a single type of cross-links,  
40 materials combining different cross-links possess desirable  
41 properties such as the ability to respond to multiple  
42 (orthogonal) stimuli, fast shape recovery, or good mechanical  
43

Received: March 2, 2020

Revised: June 19, 2020



**Figure 1.** Schematic representation of four interpenetrating polymer network (IPN) hydrogels based on different combinations of dynamic covalent bond (DCB) (acylhydrazone or oxime bond) and supramolecular interaction (metal–terpyridine bis-complexes): (a) stable DCB and long-lifetime supramolecular bond (Oxime +  $\text{Fe}^{2+}$ -Tpy), (b) stable DCB with labile supramolecular bond (Oxime +  $\text{Zn}^{2+}$ -Tpy), (c) less stable DCB with long-lifetime supramolecular bond (Acylhydrazone +  $\text{Fe}^{2+}$ -Tpy), and (d) less stable DCB with labile supramolecular bond (Acylhydrazone +  $\text{Zn}^{2+}$ -Tpy).

44 properties such as high strength, toughness, and fatigue  
45 resistance.<sup>17,20</sup>

46 As a pH-sensitive bond formed by a “click” reaction<sup>21</sup> upon  
47 condensation between a carbonyl group and an amino  
48 derivative, Schiff base bonds are one of the most successful  
49 DCBs used so far in the preparation of responsive gels.<sup>22–25</sup>  
50 Interestingly, the hydrolytic stability of Schiff base bonds can  
51 be tuned in increasing order from imine, to acylhydrazone, to  
52 oxime by changing the primary amine to a hydrazone and to a  
53 hydroxylamine.<sup>26</sup> Due to their reversibility, and greater stability  
54 than imines, acylhydrazones and oximes have been used in the  
55 synthesis of functional gels in various fields.<sup>24,27</sup> Among  
56 supramolecular interactions, the metal–terpyridine coordina-  
57 tion bond is the most attractive for the fabrication of  
58 responsive polymer gels since the bond characteristics  
59 (lifetime, strength) can be tuned over several orders of  
60 magnitudes simply by changing the metal ions used (or the  
61 ligand), it can be used in a range of solvents, and it may confer  
62 additional useful properties (catalytic, magnetic, photoactive,  
63 etc.) to the materials.<sup>28–33</sup> Therefore, in the present study, we  
64 investigate the rheological properties of polymer gels, which  
65 combine the aforementioned Schiff base bonds with metal–  
66 terpyridine coordination bonds, to create very stable—yet  
67 reversible—networks thanks to the presence of the DCBs,  
68 while keeping some room to tune the material properties,  
69 thanks to the metal–ligand interactions.

70 In general, several interactions can be combined by  
71 following either a “dual-network” approach or an “inter-  
72 penetrating polymer networks” (IPNs) approach.<sup>34</sup> A dual  
73 network is generally made of the same polymer cross-linked by  
74 two different types of bonds, often a covalent and a  
75 supramolecular bond, or two types of supramolecular  
76 bonds,<sup>20,35–37</sup> while IPNs comprise two or more interlaced  
77 polymer networks that are not covalently bonded to each  
78 other. The latter systems have gained broad interest because  
79 they allow a combination of the desired properties of each  
80 network (e.g., stimuli responsiveness), and even more, because

they may exhibit new properties that are not observed in the  
81 component networks alone.<sup>38–44</sup> Most notably, IPN hydrogels  
82 may show enhanced mechanical properties such as greater  
83 toughness, larger extensibility, and improved strength due to  
84 synergistic interactions between the component networks that  
85 transfer the stress and dissipate mechanical energy upon  
86 deformation.<sup>34,45,46</sup> Recently, the combination of DCB and  
87 supramolecular interactions has been also reported to fabricate  
88 responsive IPN hydrogels and elastomers with outstanding  
89 mechanical performances.<sup>47–53</sup> For example, Konkolewicz et  
90 al.<sup>49</sup> synthesized a double dynamic IPN elastomer with  
91 superior mechanical (increased stress and strain at break,  
92 increased malleability, greater toughness) and self-healing  
93 properties based on Diels–Alder adduct and hydrogen  
94 bonding. Liang et al.<sup>52</sup> prepared highly stretchable IPN  
95 hydrogels with the properties of actuation, shape memory,  
96 and self-healing capability using boronic ester bonds and  
97 alginate– $\text{Ca}^{2+}$  complexation.  
98

In this study, we investigate the viscoelastic properties of  
99 reversible IPN hydrogels formed through DCB and metal–  
100 ligand supramolecular interactions. In particular, we study how  
101 the rheological properties of both networks are combined and  
102 modified when these networks are interpenetrated. Since the  
103 DCBs (i.e., the acylhydrazone and oxime bonds) have been  
104 chosen to be very stable, we do not expect the samples to flow  
105 in the linear regime of deformation. However, the reversibility  
106 of the bonds could possibly be observed under large shear  
107 and/or in different environmental conditions (e.g., pH or  
108 temperature variation). On the other hand, depending on the  
109 metal ion selected, the lifetime of the supramolecular junctions  
110 can be easily varied. Therefore, the use of a supramolecular  
111 network made of labile interactions should allow us to study  
112 how the fast association/dissociation dynamics of the supra-  
113 molecular network influences the overall response of the IPN  
114 hydrogels. Then, by exploiting metal–ligand interactions with  
115 long lifetime, we would like to see how the contribution of  
116 both the DCB and supramolecular networks can be  
117

**Table 1. Main Characteristics of P(DMA-co-ketone) and P(DMA-co-Tpy) Copolymers**

copolymer	final ratio <sup>a</sup> (mol %)			$M_n^b$ (g/mol)	$M_n^c$ (g/mol)	$\bar{D}^c$	$N_f/\text{chain}^d$	
	DMA	ketone	Tpy				ketone	Tpy
P(DMA-co-ketone)	96	4		40 000	56 000	1.32	16	
P(DMA-co-Tpy)	98.5		1.5	44 000	42 500	1.73		6

<sup>a</sup>Calculated from <sup>1</sup>H NMR spectra. <sup>b</sup>Evaluated by monomer conversion (<sup>1</sup>H NMR). <sup>c</sup>Determined by SEC. <sup>d</sup>Average number of functional groups per chain.

distinguished. Finally, the cross-linking density or dynamics of the networks can be modified by varying the pH, which gives us an additional way to vary the relative stability of both networks.

To this end, we have synthesized a series of novel IPN hydrogels that are based on two functionalized hydrophilic copolymers (Figure 1). The first one bears ketone pendant groups and can be cross-linked by succinic dihydrazide or *O,O'*-(propane-1,3-diyl)bis(hydroxylamine) to form, respectively, acylhydrazone and oxime bonds, yielding Schiff base networks. The second copolymer bears terpyridine side groups and can be cross-linked by the addition of transition-metal cations ( $Zn^{2+}$  and  $Fe^{2+}$  were used in this work) to form metal-terpyridine bis-complexes. Therefore, the obtained interpenetrated networks are composed of a DCB-cross-linked network and of a supramolecularly cross-linked network. Thanks to the different nature of the cross-linkers, the bond strength and kinetic stability of the DCB (acylhydrazone or oxime) and supramolecular interaction ( $Fe^{2+}$ -terpyridine or  $Zn^{2+}$ -terpyridine bis-complexes) can be independently tuned. As shown in Figure 1, four IPN hydrogels have thus been obtained by combining these interactions in different ways. First, a very stable (i.e., characterized by a high equilibrium constant) DCB is combined with a long-lifetime supramolecular interaction (Oxime +  $Fe^{2+}$ -Tpy) or with a more dynamic supramolecular interaction (Oxime +  $Zn^{2+}$ -Tpy). Second, a less stable DCB is combined with the long-lifetime supramolecular interaction (Acylhydrazone +  $Fe^{2+}$ -Tpy) or with the more dynamic supramolecular interaction (Acylhydrazone +  $Zn^{2+}$ -Tpy). The influence of these different combinations of interactions on the IPN properties is investigated in detail by rheology.

## RESULTS AND DISCUSSION

### Synthesis of Hydrophilic-Functionalized Copolymers.

We have chosen the hydrophilic biocompatible poly(*N,N*-dimethyl acrylamide) (PDMA) as the backbone polymer for fabricating the hydrogels. The commercially available comonomer, diacetone acrylamide (DAAM), which contains a ketone group that can react with dihydrazide or bishydroxylamine compounds to form acylhydrazone or oxime bonds, was employed to create Schiff base bond-based networks (Figure 1). The hydrophilic terpyridine-functionalized monomer (*N*-(2-(2-([2,2':6,2''-terpyridine]-4'-yloxy)ethoxy)ethyl)-acrylamide (TPy-DEG-AM)) was synthesized in two steps from commercially available precursors (see the Supporting Information) and can form metal-terpyridine bis-complexes with various strengths and labilities in combination with transition-metal ions. The copolymers that will be the precursors of the network were prepared by copolymerizing functionalized monomers, i.e., one bearing a ketone group and the other bearing a terpyridine, with the base monomer of DMA. Reversible addition-fragmentation chain transfer (RAFT)-controlled radical polymerization was used to this

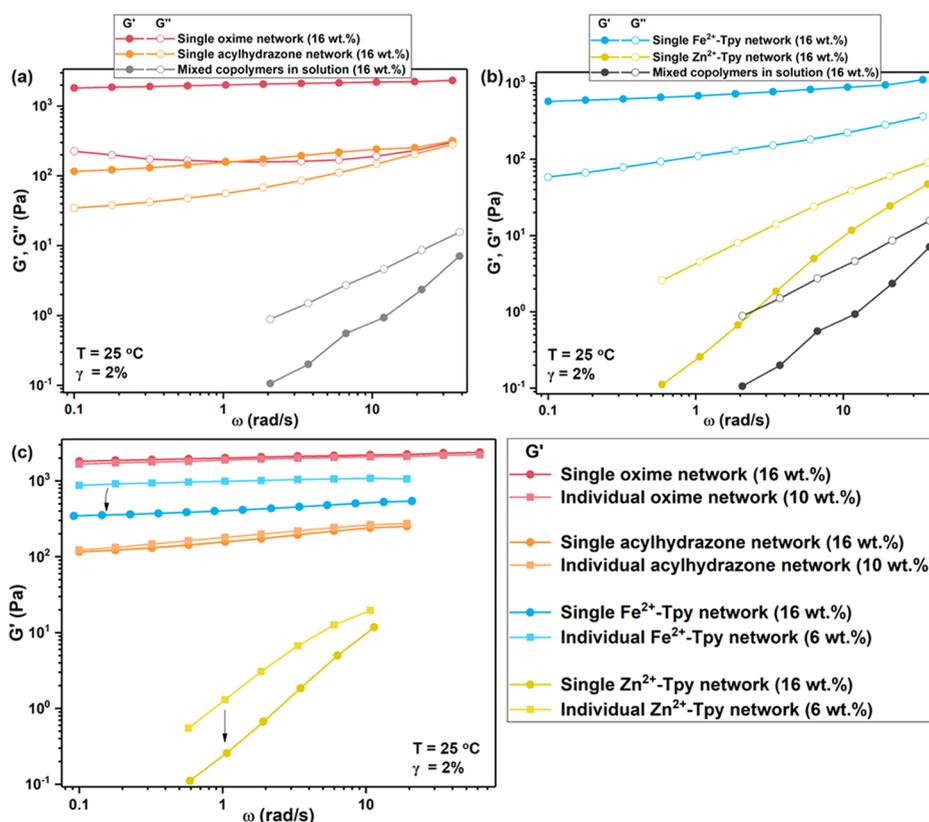
aim. Two copolymers, P(DMA-co-ketone) and P(DMA-co-Tpy), were obtained in this way and were characterized by NMR and size-exclusion chromatography (SEC) (Table 1).

**Preparation of Networks.** The P(DMA-co-ketone) copolymer was used as a precursor for preparing acylhydrazone/oxime networks, and the P(DMA-co-Tpy) copolymer was used for the formation of metal-ligand networks. For all of the prepared networks, the amount of added cross-linkers (dihydrazides, bishydroxylamines, or transition-metal cations) was half an equivalent compared to the reaction sites (ketone groups or terpyridine groups) of the copolymers. Three types of networks of increasing complexity were prepared to allow the systematic comparison of their rheological properties and the determination of the respective contributions of the two types of bonds. Individual networks were prepared from each of the above copolymers with corresponding cross-linkers (Schemes S5 and S6). Single networks were prepared from mixed solutions of the two copolymers but cross-linking only one of the copolymers with the appropriate cross-linker (Scheme S7). Interpenetrating polymer networks were prepared also from mixed solutions of the two copolymers, but this time cross-linking both copolymers (Scheme S8).

Formation of individual networks from each of the two above copolymers has been first investigated in deionized water (pH: 6–7). We found that the P(DMA-co-ketone) copolymer reacts with the dihydrazide cross-linker to form acylhydrazone hydrogels after 1 day, and with bishydroxylamine cross-linker to form oxime hydrogels after 9 h at a copolymer concentration of 10 wt %. At lower concentrations, P(DMA-co-ketone) cannot form gels with these cross-linkers even after 1 month of reaction. The P(DMA-co-Tpy) copolymer is cross-linked by  $Fe^{2+}$  ions in a few minutes via the formation of  $Fe^{2+}$ -terpyridine bis-complexes ( $Fe^{2+}$ -Tpy) at a minimum copolymer concentration of 6 wt %. Therefore, concentrations of 10 wt % for the P(DMA-co-ketone) copolymer and of 6 wt % for the P(DMA-co-Tpy) copolymer have been adopted in this work for network preparation. In addition, two single networks were also prepared at a total polymer concentration of 16 wt % by mixing both copolymers together, 10% of P(DMA-co-ketone), and 6% of P(DMA-co-Tpy), but inducing the cross-linking of only one of the copolymers with the appropriate reagent.

The IPN hydrogels were prepared by adding dihydrazide or bishydroxylamine and metal ions ( $Zn^{2+}$  or  $Fe^{2+}$ ) to solutions of mixed copolymers: 10 wt % P(DMA-co-ketone) and 6 wt % P(DMA-co-Tpy) to reach a total polymer concentration of 16 wt % as for the single networks. The influence of the addition sequence of cross-linkers, i.e., inducing first the DCB formation and then the metal-ligand bonds or the reverse, on the rheological properties of the obtained IPNs was studied. In each case, a 24 h waiting time was applied before adding the second cross-linker.

**Rheological Characterization.** Oscillatory shear rheology was used as the main characterization method to investigate



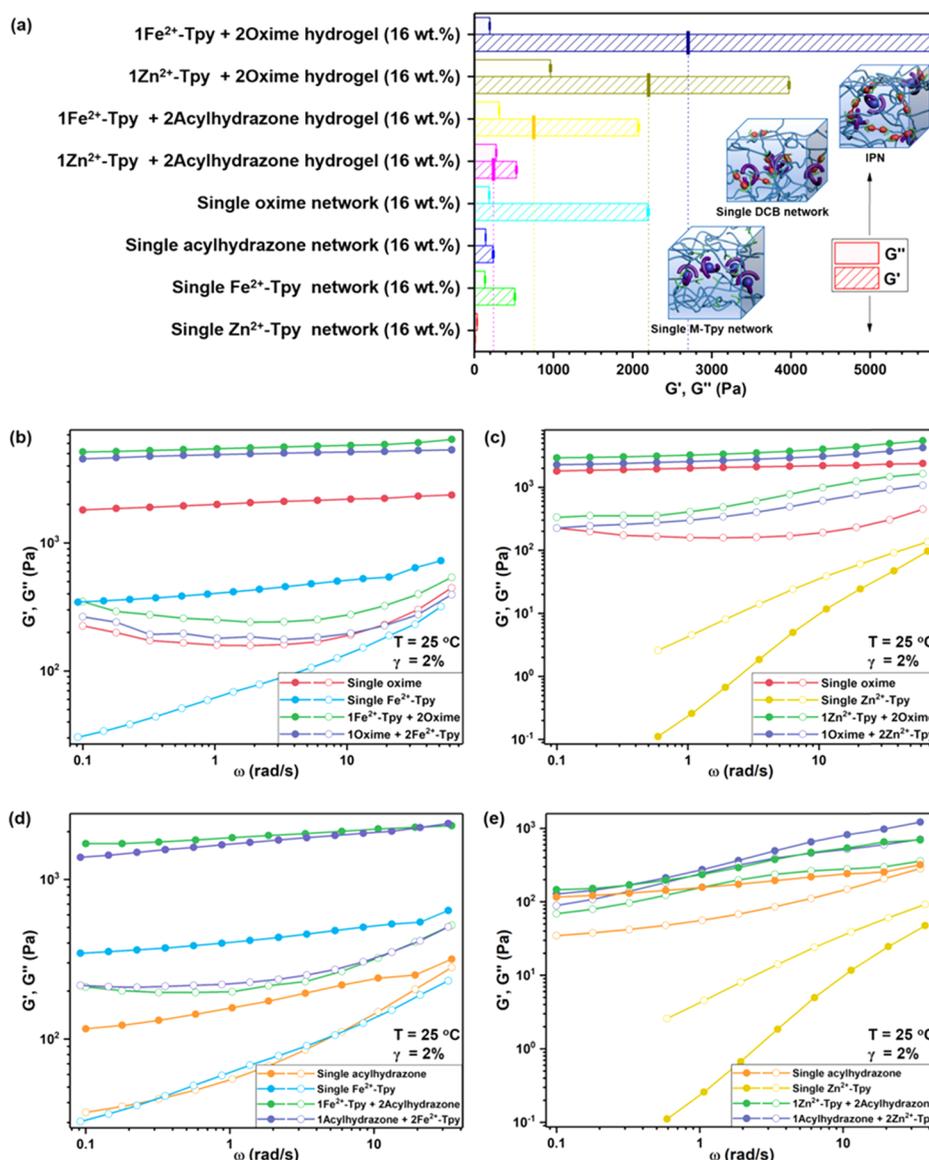
**Figure 2.** Oscillatory frequency sweeps on single networks based on (a) acylhydrazone and oxime and (b) on  $\text{Fe}^{2+}$ -Tpy and  $\text{Zn}^{2+}$ -Tpy from the mixed copolymer solution of P(DMA-*co*-ketone) and P(DMA-*co*-Tpy). (c) Comparison of the storage modulus of individual and single networks of oxime, acylhydrazone,  $\text{Fe}^{2+}$ -Tpy, and  $\text{Zn}^{2+}$ -Tpy.

225 the dynamic mechanical properties of all networks under shear.  
 226 The dynamic covalent bonds generally exhibit higher bond  
 227 dissociation energies and slower dynamics than supramolecular  
 228 interactions.<sup>12,17</sup> In our case, the order of rate constants for the  
 229 formation of cross-links between two chains is approximately  
 230 acylhydrazone < oxime <  $\text{Zn}^{2+}$ -Tpy <  $\text{Fe}^{2+}$ -Tpy at 25 °C in  
 231 water (pH ~ 7).<sup>54–58</sup> Therefore, we first measured the  
 232 oscillatory shear rheological behavior of the individual  
 233 acylhydrazone hydrogel, i.e., the slowest-forming network  
 234 according to the above data, at different aging times to  
 235 determine the best preparation time to achieve stable and  
 236 reproducible frequency sweeps. Amplitude sweep measure-  
 237 ments were also performed to determine the limit of the linear  
 238 regime of deformation. As depicted in Figure S3, the  
 239 rheological behavior of individual acylhydrazone hydrogels  
 240 did not change significantly after 2 days of aging, indicating  
 241 that a stable state has been reached. Based on these results, all  
 242 of the following rheology measurements on all hydrogels have  
 243 been executed after 2 days of aging time at room temperature.  
 244 The dynamic viscoelastic behaviors of individual networks of  
 245 oxime, acylhydrazone,  $\text{Fe}^{2+}$ -Tpy, and  $\text{Zn}^{2+}$ -Tpy were  
 246 measured by oscillatory frequency sweeps (Figure S4). For  
 247 these four samples, the storage moduli ( $G'$ ) are always higher  
 248 than their pure copolymer solutions, indicating the formation  
 249 of cross-links after 2 days of aging.<sup>1</sup> H NMR characterizations  
 250 (Figure S5) also proved the formation of oxime and  
 251 acylhydrazone cross-links. The storage moduli of the  
 252 acylhydrazone, oxime, and  $\text{Fe}^{2+}$ -Tpy samples are almost  
 253 constant over the whole experimental frequency window,  
 254 showing that stable gels have been formed. Their values, which

are close to 1 kPa for oxime and  $\text{Fe}^{2+}$ -Tpy, and close to 200  
 255 Pa for acylhydrazone, can be compared to the values found if  
 256 we assume that all of the functional groups lead to the creation  
 257 of effective intermolecular cross-links, i.e.,  

$$G_N^0 = \frac{\rho_0 RT}{M_{XX}} (1 - \varphi_{\text{dangling}})$$
 where  $\rho_0$  is the density of PDMA  
 in the melt state (approximated as 1 g/cm<sup>3</sup>),  $c$  is the sample  
 259 concentration,  $M_{XX}$  is the average molar mass between two  
 260 sticky groups (estimated to be 2.5 kg/mol for P(DMA-*co*-  
 261 ketone) and 7.3 kg/mol for P(DMA-*co*-  
 262 Tpy); see Table 1),  
 263 and  $\varphi_{\text{dangling}}$  is the weight fraction of dangling ends, which do  
 264 not participate in the network elasticity and can be  
 265 approximated as equal to  $2M_{XX}/M_w$ . In such a case, the  
 266 plateau moduli of the P(DMA-*co*-  
 267 Tpy) samples should be approximately equal to 89 and 16 kPa,  
 268 respectively, which are much higher than the values found  
 269 experimentally. This result suggests the presence of a large  
 270 number of unreacted groups, as well as the presence of internal  
 271 loops due to intramolecular cross-links that do not contribute  
 272 to the sample elasticity, especially in the case of the  
 273 acylhydrazone network. The higher level of the plateau  
 274 modulus of the oxime network is due to a higher cross-linking  
 275 density of oxime hydrogels, consistent with the greater  
 276 equilibrium constant and the greater intrinsic hydrolytic  
 277 stability of oximes compared to acylhydrazones.<sup>58</sup>

On the other hand, the relatively higher level of the rubbery  
 278 plateau observed for the  $\text{Fe}^{2+}$ -Tpy system (compared to the  
 279 value found in the case of the perfect network) demonstrates  
 280 its larger capability to create intermolecular junctions. This can  
 281 be due to both the high association constant of  $\text{Fe}^{2+}$ -  
 282 terpyridine bis-complexes<sup>54</sup> and the fact that the molecular 283



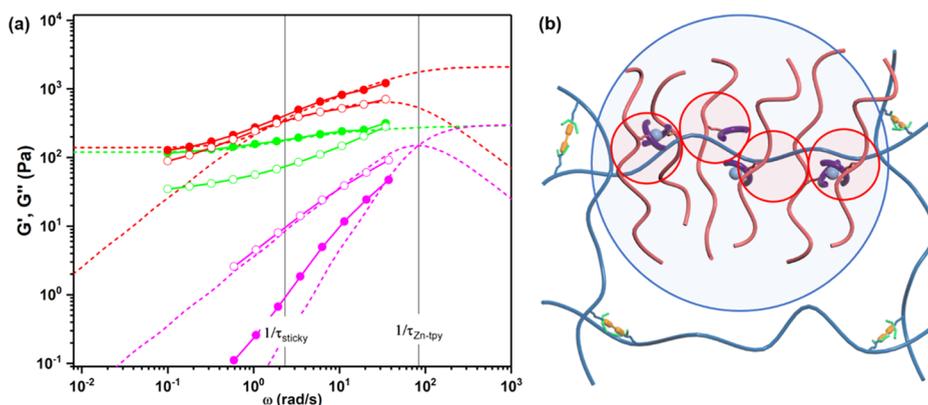
**Figure 3.** (a) Summary of the dynamic moduli values for the different IPN hydrogels and the corresponding single networks. The values were obtained from the frequency sweeps at a frequency of 10 rad/s. The vertical lines on the  $G'$  bar of the four IPN hydrogels represent the sum of the  $G'$  of the corresponding single networks. (b–e) Oscillatory frequency sweeps on the IPN hydrogels and their corresponding single networks ( $G'$ : filled symbols,  $G''$ : open symbols). The numbers 1 and 2 in the sample names refer to the addition sequence of the cross-linkers.

284 strands between two sticky groups are longer, which reduces  
 285 the probability of creating internal loops. Only the system  
 286 based on Zn<sup>2+</sup>-Tpy associations is able to flow within the  
 287 experimental frequency window. This is attributed to the lower  
 288 equilibrium constant and high lability of Zn<sup>2+</sup>-terpyridine bis-  
 289 complexes,<sup>54</sup> which largely reduce the lifetime of the  
 290 supramolecular network.<sup>28</sup> Moreover, at a high frequency, a  
 291 power law of 1/2 is found for  $G'(\omega)$ , indicating that before the  
 292 terminal regime, the relaxation of this material is well described  
 293 by a (constraint release) Rouse process.

294 Next, the possible influence of free chains (non-cross-linked)  
 295 of the other copolymer type on the network properties is  
 296 investigated, as shown in Figure 2a,b. These single networks  
 297 contain 10 wt % P(DMA-*co*-ketone) and 6 wt % P(DMA-*co*-  
 298 Tpy) and only one type of cross-linker. Figure 2c compares  
 299 their storage moduli to the ones of their individual networks. It  
 300 is seen that the viscoelastic response of the acylhydrazone and  
 301 oxime samples is not influenced by the presence of P(DMA-*co*-

Tpy) chains, which suggests that there is no interaction  
 302 between P(DMA-*co*-ketone) and P(DMA-*co*-Tpy) chains  
 303 when the P(DMA-*co*-ketone) copolymer is cross-linked in  
 304 the presence of the other copolymer type. This also highlights  
 305 the fact that the unassociated chains (or dangling ends) are  
 306 relaxing very fast compared to the lifetime of the associated  
 307 dynamic covalent interactions and do not contribute to the  
 308 sample elasticity in the frequency window measured  
 309 experimentally.

310 In the case of the supramolecular networks (Fe<sup>2+</sup>-Tpy and  
 311 Zn<sup>2+</sup>-Tpy), the comparison between the dynamic mechanical  
 312 properties of their single and individual supramolecular  
 313 networks shows that mixing the two copolymers slightly  
 314 reduces the level of the elastic modulus. The reason behind  
 315 this could be a “screening effect” induced by the presence of a  
 316 large amount of the nonactive P(DMA-*co*-ketone) copolymer  
 317 compared to the P(DMA-*co*-Tpy) copolymer (10 vs 6%),  
 318 slightly reducing the proportion of associated stickers or  
 319



**Figure 4.** (a) Experimental (symbols) and theoretical (dashed curves) storage (full symbols) and loss moduli (empty symbols) of the single  $\text{Zn}^{2+}$ -Tpy network (magenta), the single acylhydrazone network (green), and the 1Acylhydrazone +  $2\text{Zn}^{2+}$ -Tpy IPN (red). (b) Cartoon representing the sticky Rouse relaxation of the molecular segments in the acylhydrazone network (represented in blue). While at very short times, interactions with the  $\text{Zn}^{2+}$ -Tpy network (in red) prevent the motion of these segments (see the red blobs), at longer times, the segments are able to explore a larger surrounding (see the blue blob) and partially relax, at the rhythm of dissociations–associations of the  $\text{Zn}^{2+}$ -Tpy network.

320 promoting the formation of internal loops and therefore  
321 affecting the, already low, cross-linking density of  $\text{Fe}^{2+}$ -Tpy  
322 and  $\text{Zn}^{2+}$ -Tpy.

323 Knowing the dynamics of the single networks, we can now  
324 investigate the viscoelastic properties of the four IPN  
325 hydrogels, which are presented in Figure 3. There are several  
326 points to highlight here. First, as for the single networks, the  
327 frequency dependence of the storage modulus of most of the  
328 IPNs is very limited, showing only a weak decrease with  
329 decreasing frequency, indicating that stable gels have been  
330 formed. As expected, the storage modulus measured at 10 rad/  
331 s,  $G'(\omega = 10 \text{ rad/s})$ , is larger for the IPN containing the more  
332 stable bonds, i.e.,  $1\text{Fe}^{2+}$ -Tpy +  $2\text{Oxime}$ , with  $G'(\omega = 10 \text{ rad}/$   
333  $\text{s}) = 5780 \text{ Pa}$ . The modulus then takes lower value for the IPNs  
334  $1\text{Zn}^{2+}$ -Tpy +  $2\text{Oxime}$  (3975 Pa) and  $1\text{Fe}^{2+}$ -Tpy +  
335  $2\text{Acylhydrazone}$  (2072 Pa) and becomes very small for the  
336 IPN  $1\text{Zn}^{2+}$ -Tpy +  $2\text{Acylhydrazone}$  (532 Pa). The latter value  
337 is not representative of the plateau modulus since it is taken in  
338 the flow regime of the sample. Furthermore, it is observed that  
339 the addition order of the two cross-linkers has a slight  
340 influence on the dynamic mechanical properties of the IPNs.  
341 For the systems with at least one long lifetime cross-link type,  
342 i.e.,  $\text{Fe}^{2+}$ -Tpy + Oxime,  $\text{Zn}^{2+}$ -Tpy + Oxime, and  $\text{Fe}^{2+}$ -Tpy +  
343 Acylhydrazone (Figure 3b–d), adding first the metal ions  
344 ( $\text{Zn}^{2+}$ ,  $\text{Fe}^{2+}$ ) to build the supramolecular network, followed by  
345 the addition of dihydrazide/bishydroxylamine to create the  
346 second network yields IPNs with slightly higher moduli. This  
347 could come from the greater chain mobility of the P(DMA-*co*-  
348 ketone) copolymer inside the more sparsely cross-linked  
349 supramolecular first network, compared to the reverse cross-  
350 linking order where the denser DCB network is formed first,  
351 allowing a slightly easier and more efficient formation of the  
352 second network. On the other hand, the less stable DCB with  
353 labile metal–ligand bond (Acylhydrazone +  $\text{Zn}^{2+}$ -Tpy)  
354 system shows the opposite behavior, the dynamic moduli of  
355 the IPN being higher when the acylhydrazone cross-links are  
356 formed before the  $\text{Zn}^{2+}$ -Tpy cross-links (Figure 3e). This  
357 could be explained by the fact that the viscoelastic response of  
358 the IPN in which  $\text{Zn}^{2+}$ -Tpy cross-links are formed first does  
359 not easily reach its equilibrium state, as confirmed by Figure  
360 S6, which shows that the moduli of this IPN reach the same  
361 level as for the other one after 1 month of aging.

An interesting point to observe in Figure 3 is the fact that 362  
the storage modulus of each IPN hydrogel is higher than the 363  
sum of their single network hydrogels. For example, the sum of 364  
the storage modulus of the single  $\text{Fe}^{2+}$ -Tpy hydrogel (511 Pa) 365  
and oxime hydrogel (2194 Pa) is only equal to 2705 Pa, which 366  
is much lower than that of the corresponding IPN hydrogel 367  
(5780 Pa). These results indicate a synergetic behavior 368  
between the two interpenetrating networks which stiffens the 369  
IPN hydrogels beyond the simple sum of the moduli (Figure 370  
3a). This enhanced modulus of IPN hydrogels most probably 371  
arises from the fact that part of the entanglements created 372  
between the P(DMA-*co*-ketone) and P(DMA-*co*-Tpy) chains 373  
due to the two cross-linked networks can now be trapped 374  
between associated stickers, and therefore act as additional 375  
physical interactions governed by the dynamics of the stickers. 376  
Thus, the IPN elasticity is not only due to the associated 377  
reversible junctions but also due to the possible interactions 378  
between the chains. 379

While the influence of blending two networks on the sample 380  
elasticity is clearly observed in Figure 3a, it is also important to 381  
investigate how it influences the relaxation dynamics of the 382  
IPN. To this end, we focus on the IPN containing  $\text{Zn}^{2+}$ -Tpy 383  
junctions since the relaxation of the complexes is fast enough 384  
to be measured under the conditions used here. The  $\text{Zn}^{2+}$ - 385  
Tpy + Acylhydrazone IPN shows the strongest frequency 386  
dependence since it is made of the two weakest bonds (Figure 387  
3e). The decrease of  $G'$  with frequency for this IPN is 388  
proportionally more pronounced than for the acylhydrazone 389  
single network, showing that this decrease is mainly due to the 390  
relaxation of the  $\text{Zn}^{2+}$ -Tpy network, which allows in turn the 391  
release of both the supramolecular network elasticity and the 392  
interactions between the two networks. As shown in Figure 4, 393  
we also observe that the relaxation of the  $\text{Zn}^{2+}$ -Tpy network 394  
within this IPN starts at a time similar to the relaxation time of 395  
the single  $\text{Zn}^{2+}$ -Tpy network. However, a much longer time is 396  
required before the contribution of the  $\text{Zn}^{2+}$ -Tpy network 397  
fully vanishes and the IPN reaches the modulus of the 398  
acylhydrazone single network. In the transition zone between 399  
these two times, a characteristic slope of  $-1/2$  is observed in 400  
the storage modulus, indicating a Rouse relaxation. This result 401  
can be understood as follows: the IPN elasticity mostly arises 402  
from the interactions between the two networks. With time, 403  
since the  $\text{Zn}^{2+}$ -Tpy complexes of the supramolecular network 404

405 continuously dissociate and associate, the molecular segments  
 406 located between two DCBs of the acylhydrazone network are  
 407 able to explore their surrounding, but only at the rhythm of the  
 408 relaxation (or association/dissociation dynamics) of the  
 409 supramolecular bonds (see Figure 4b). Therefore, this slow  
 410 (and partial) relaxation of the acylhydrazone network segments  
 411 is well described by a sticky Rouse process<sup>59,60</sup>

$$G(t) = G_N^0 \phi(t) + G_N^0 \sum_{p=1}^{N_{Zn-Tpy}} \exp\left(\frac{-p^2 t}{\tau_{Zn-Tpy} N_{Zn-Tpy}}\right) \quad (1)$$

413 where  $G_N^0$  is the plateau modulus of the acylhydrazone  
 414 network,  $\phi(t)$  is the fraction of the acylhydrazone network  
 415 which is not relaxed at time  $t$ ,  $N_{Zn-Tpy}$  is the number of  
 416 interactions between the acylhydrazone and  $Zn^{2+}$ -Tpy  
 417 networks located between two associated DCBs, and  $\tau_{Zn-Tpy}$   
 418 is the average lifetime of the  $Zn^{2+}$ -Tpy network. This model is  
 419 tested in Figure 4a, in which we consider that  $\tau_{Zn-Tpy} = 0.012$  s  
 420 (as determined by approximating the viscoelastic response of  
 421 the single network by a single Maxwell mode),  $G_N^0 = 300$  Pa (as  
 422 observed experimentally), and considering a stretched  
 423 exponential function to approximate the relaxation function  
 424  $\phi(t)$  of the single acylhydrazone network (green curve),  $\phi(t) =$   
 425  $0.5 + 0.5 \exp(-t^{0.5})/0.45$ .

426 The only unknown parameter is the number of network–  
 427 network interactions per segment of the acylhydrazone  
 428 network, which determines both the level of the high-  
 429 frequency rubbery plateau of the IPN and the time needed  
 430 for the influence of the  $Zn^{2+}$ -Tpy network to disappear. This  
 431 number must be fixed to 6 to correctly describe the  
 432 experimental data (Figure 4a).

433 These results suggest that the partial relaxation of the long-  
 434 lifetime network takes place through sticky Rouse relaxation  
 435 process. This means that the time needed to recover the same  
 436 elasticity as in the single, long-lifetime network,  $\tau_{sticky}$  is  
 437  $N_{Zn-Tpy}^2$  times longer than the lifetime of the short-lifetime  
 438 network.

439 A short comment should be made here. Usually, sticky  
 440 Rouse relaxation is observed with dual networks<sup>61</sup> and not with  
 441 interpenetrated networks. To be exact, one could argue that  
 442 the Rouse regime observed in Figure 4a is not a sticky Rouse  
 443 process, but rather a constraint release Rouse regime, where  
 444 the molecular segments of the acylhydrazone network partially  
 445 relax thanks to the disentanglement and relaxation of the  
 446  $Zn^{2+}$ -Tpy network, as described in ref 62. However, since the  
 447 relaxation of the  $Zn^{2+}$ -Tpy network is fully governed by the  
 448 relaxation of the supramolecular complexes, it seems  
 449 appropriate to define this Rouse regime by a sticky Rouse  
 450 relaxation.

451 The viscoelastic response of the 1Oxime + 2 $Zn^{2+}$ -Tpy IPN  
 452 can also be modeled based on eq 1 (Figure 5). In this case, we  
 453 consider the same relaxation time  $\tau_{Zn-Tpy}$  as with the  
 454 1Acylhydrazone + 2 $Zn^{2+}$ -Tpy IPN since the oxime network  
 455 is diluted in the same short-lifetime network. Furthermore, the  
 456 plateau modulus of the single oxime network is fixed from the  
 457 experimental data as equal to 2100 Pa, while the function  $\phi(t)$   
 458 is well approximated by  $\phi(t) = 1$ . The number of interactions  
 459 per molecular segment between the two networks is, again,  
 460 determined by best fitting. We find that ( $N_{Zn-Tpy} = 2$ ) leads to  
 461 a good agreement between the theoretical and the  
 462 experimental data (Figure 5). This lower value is a direct  
 463 consequence of the fact that the oxime network is much denser  
 464 than the acylhydrazone network. Therefore, the molecular

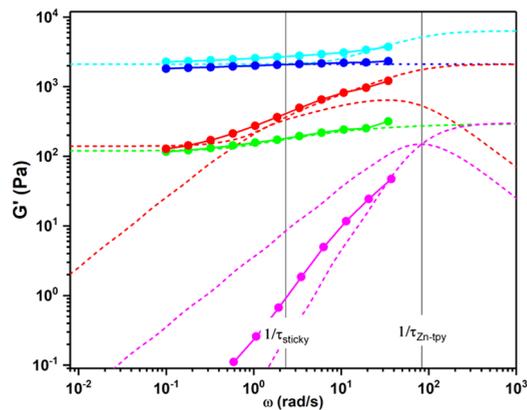


Figure 5. Experimental (symbols) and theoretical (dashed curves) storage modulus of the single  $Zn^{2+}$ -Tpy network (magenta), the single acylhydrazone network (green), 1Acylhydrazone + 2 $Zn^{2+}$ -Tpy IPN (red), single oxime network (blue), and 1Oxime + 2 $Zn^{2+}$ -Tpy IPN (cyan).

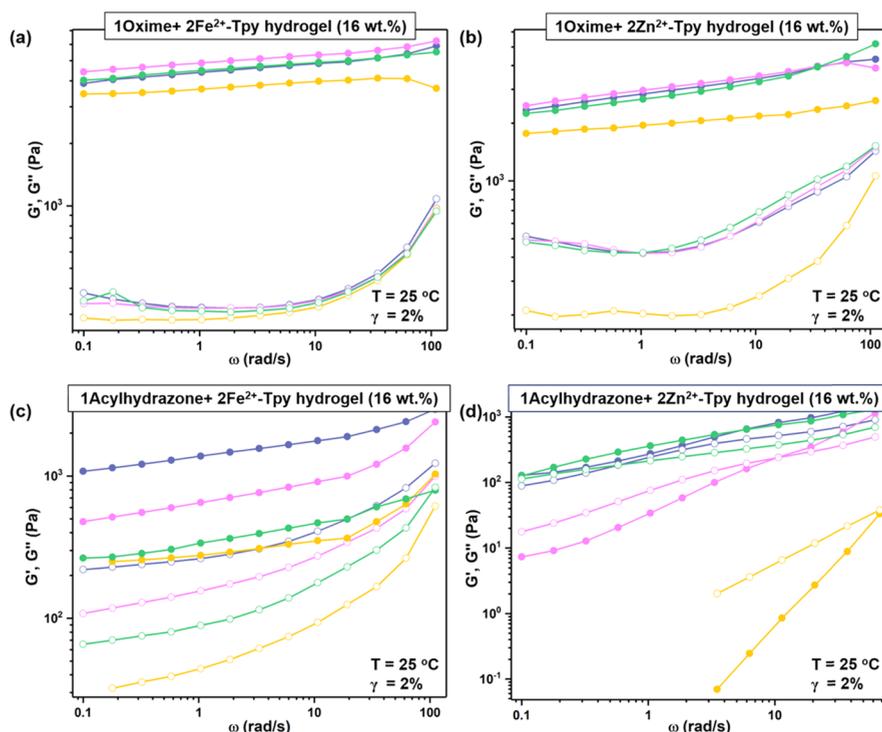
segments between two associated DCBs are shorter, which  
 465 limits the number of interactions with the  $Zn^{2+}$ -Tpy network.  
 466

When  $Fe^{2+}$  ions are used instead of  $Zn^{2+}$  in the  
 467 supramolecular network, the lifetime of the complexes  
 468 becomes too long to easily observe its relaxation. As shown  
 469 in Figure S7, the loss modulus of the single  $Fe^{2+}$ -Tpy network  
 470 only starts to increase at a frequency of around 0.01 rad/s,  
 471 which indicates the beginning of the network relaxation.  
 472 Nevertheless, the data suggest that, similarly to the  
 473 1Acylhydrazone + 2 $Zn^{2+}$ -Tpy IPN, partial relaxation of the  
 474 1Acylhydrazone + 2 $Fe^{2+}$ -Tpy IPN starts to take place at a  
 475 time equal to the lifetime of the complexes, followed by a  
 476 Rouse-like relaxation. This behavior is thus similar to the one  
 477 with the  $Zn^{2+}$ -Tpy complexes, but it is slowed down by  
 478 around 3 orders of magnitude.  
 479

To speed up the partial relaxation of these IPNs, external  
 480 conditions must be changed. In the following, we investigate  
 481 the influence of a reduced pH on the dynamics of the IPN  
 482 hydrogels. Indeed, as mentioned in the Introduction section,  
 483 due to the fact that Schiff base bonds are pH-sensitive<sup>58</sup> and  
 484 that the protonation of the terpyridine ligand weakens the  
 485 metal–terpyridine coordination bonds,<sup>63</sup> the IPN hydrogels  
 486 are expected to have the ability of gel–sol transition by  
 487 changing the pH of the environment. To study the pH  
 488 responsiveness of the prepared IPN hydrogels, HCl (2 M) and  
 489 triethyl-amine were used as pH regulators. As mentioned  
 490 above, all IPN hydrogels were prepared from pure water at pH  
 491 6–7.  
 492

Figure 6 presents the rheology data on the four IPNs at  
 493 different pH values. Most IPN hydrogels stay in the gel state  
 494 even at low pH (Figure 6a–c), apart from the Acylhydrazone +  
 495  $Zn^{2+}$ -Tpy IPN, made of the two weakest bonds, which turns  
 496 into a solution at pH 1–2, showing that both subnetworks  
 497 have been fully destructured (Figure 6d). The oxime-based  
 498 IPN hydrogels (Figure 6a,b) and the corresponding individual  
 499 oxime network (Figure S8a) are least affected by the pH  
 500 change. This difference compared to the acylhydrazone-based  
 501 systems (Figure 6c,d) can be attributed to the higher resistance  
 502 toward hydrolysis of oxime compared to acylhydrazone  
 503 bonds.<sup>26,58,64</sup>  
 504

We also observe that the individual network based on  $Fe^{2+}$ -  
 505 Tpy complexes (Figure S9a) is more affected by pH than the  
 506 individual oxime network (Figure S8a), as can be seen by the  
 507



**Figure 6.** pH dependence of the dynamic moduli ( $G'$ : filled symbols,  $G''$ : empty symbols) of the IPN hydrogels. Blue curves: initial hydrogel at pH 6–7, pink curves: pH 3–4, yellow curves: pH 1–2, green curves: back to pH 6–7.

508 drop of modulus by a factor of around 2.5 at pH 1–2,  
 509 indicating that a lower number of complexes are formed at this  
 510 pH. However, even at pH 1–2, this sample still displays a  
 511 second, low-frequency plateau, which can be attributed to the  
 512 long relaxation time of the supramolecular complexes. The  
 513 influence of pH is much more important for the 1Acylhydrazone +  
 514 2Fe<sup>2+</sup>–Tpy IPN since low pH completely fluidizes  
 515 the acylhydrazone individual network (Figure S8b). Therefore,  
 516 at low pH, the contribution of acylhydrazone to the IPN is  
 517 only observed at a high frequency and vanishes at longer time,  
 518 at which the IPN behaves similarly to the individual Fe<sup>2+</sup>–Tpy  
 519 network, i.e., as if the acylhydrazone network was not present.  
 520 Playing with the pH is thus a way to promote the reversible  
 521 dynamics of this IPN, otherwise too stable at neutral pH. In  
 522 particular, at low pH, it is the DCB network that is relaxing  
 523 first, not the Fe<sup>2+</sup>–Tpy supramolecular network as it is the case  
 524 at neutral pH (see Figure S7).

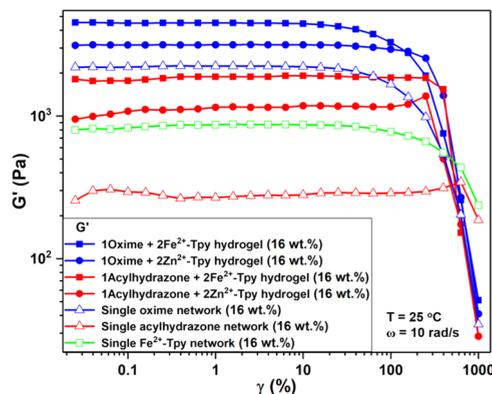
525 For the two other IPNs (Figure 6b,d), the association  
 526 dynamics of the Zn<sup>2+</sup>–Tpy network is always much faster than  
 527 that of both DCB networks. Therefore, at a low frequency, the  
 528  $G'$  and  $G''$  moduli of the Acylhydrazone + Zn<sup>2+</sup>–Tpy and  
 529 Oxime + Zn<sup>2+</sup>–Tpy IPNs are similar to the ones of the DCB  
 530 individual network, showing that the Zn<sup>2+</sup>–Tpy network is  
 531 completely destructured and only the acylhydrazone and oxime  
 532 networks partially remain (Figure S8).

533 From Figure 6, we also note that three out of the four IPN  
 534 hydrogels show complete recovery when the pH is returned to  
 535 its original value. Only the Acylhydrazone + Fe<sup>2+</sup>–Tpy IPN  
 536 cannot recover its original state. This may be explained by the  
 537 fact that for this IPN, the supramolecular bonds (Fe<sup>2+</sup>–Tpy)  
 538 are more stable than the acylhydrazone bonds and are thus  
 539 dominant in the viscoelastic response. Since these bonds are  
 540 quite sensitive to pH, as shown in Figure S9a for the Fe<sup>2+</sup>–Tpy  
 541 individual network, a significant part of these bonds dissociates

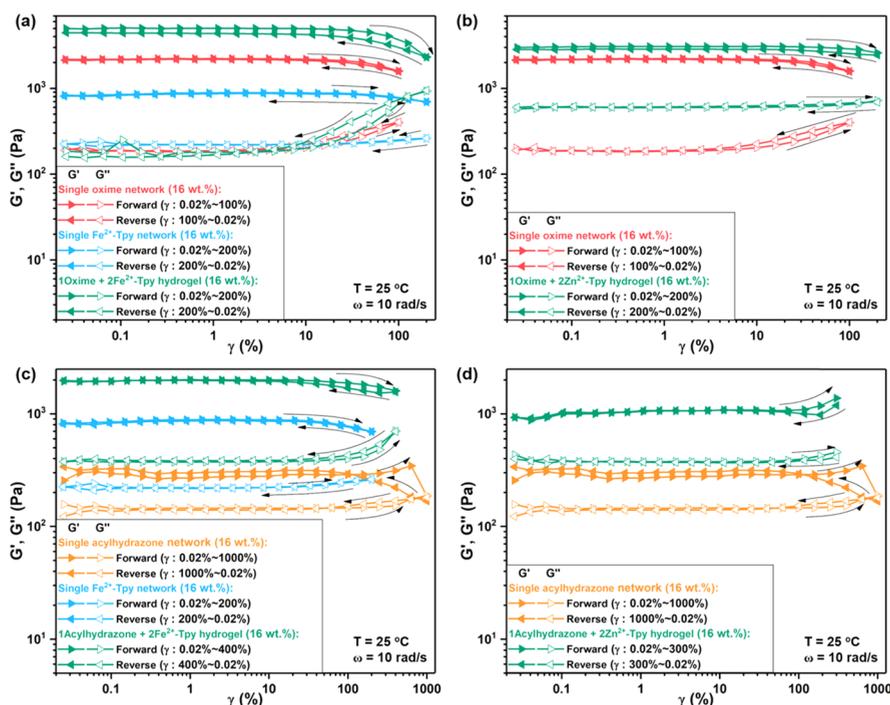
at a low pH, leading to a decrease of the plateau modulus, as  
 542 observed in Figure 6c. When the pH is set back to the original  
 543 value, the Fe<sup>2+</sup>–Tpy complexes re-form rapidly but in a less  
 544 optimal configuration, yielding a network with a lower degree  
 545 of cross-linking. The optimal reorganization of this “frozen”  
 546 network is strongly limited due to the low lability of the Fe<sup>2+</sup>–  
 547 Tpy complexes.

548  
 549 These results show that the rheological properties of the  
 550 IPN hydrogels can be finely tuned by changing the pH and  
 551 that the pH sensitivity and reversibility of the gel–sol  
 552 transition depends strongly on the combination of interactions  
 553 used to build the IPNs.

554 Finally, we study the behavior of the single networks and  
 555 IPNs under large deformation by performing strain sweeps  
 556 (Figure 7). The three single networks (the Zn<sup>2+</sup>–Tpy sample



**Figure 7.** Oscillatory strain sweeps performed on the four IPN hydrogels and the single networks. The single Zn<sup>2+</sup>–Tpy sample is not shown because it is completely relaxed under these conditions due to its fast dynamics.



**Figure 8.** Oscillatory reversible strain sweeps performed on the different IPNs and their corresponding single networks: (a) 1Oxime + 2Fe<sup>2+</sup>-Tpy I, (b) 1Oxime + 2Zn<sup>2+</sup>-Tpy, (c) 1Acylhydrazone + 2Fe<sup>2+</sup>-Tpy, and (d) 1Acylhydrazone + 2Zn<sup>2+</sup>-Tpy.

557 is not shown since its dynamics is too fast) show a constant  
 558 elastic modulus over a rather large strain range indicative of an  
 559 extended linear deformation regime. The critical strain value,  
 560 marking the end of the linear regime, increases in the order  
 561 oxime, Fe<sup>2+</sup>-Tpy, acylhydrazone, following the decrease of  
 562 cross-linking density in these three networks. At large strain  
 563 amplitudes, the networks cannot withstand the deformation  
 564 anymore and the samples break and are expelled from the  
 565 geometries. Therefore, to probe the reversibility of the bonds,  
 566 measurements were performed from low strain up to the  
 567 maximum strain amplitude that can be reached without  
 568 destroying the sample, then from this high strain amplitude  
 569 down to low strain. Under such conditions, all of the single  
 570 networks fully recover their original state, as shown in Figure 8.  
 571 The small hysteresis that is observed for the highly sheared  
 572 samples is attributed to the strain-induced breaking of part of  
 573 the reversible bonds, the latter being able to re-form when the  
 574 deformation amplitude is reduced.

575 For the single acylhydrazone network, a slight shear  
 576 thickening effect is observed at a high shear amplitude. Such  
 577 behavior has already been reported in the literature for  
 578 reversible networks and can be attributed to the fact that large  
 579 shear flow promotes the formation of intermolecular  
 580 associations.<sup>65,66</sup> While other mechanisms could also lead to  
 581 shear thickening (such as chain stretching), an increase of  
 582 intermolecular associations fits our results since when going  
 583 back from high to low strain amplitude, the storage and loss  
 584 moduli of this network are slightly higher than the  
 585 corresponding initial values (Figure 8c,d), indicating a better  
 586 organization of the network. This shear thickening property is  
 587 observed only for the acylhydrazone network, which contains a  
 588 large amount of nonactive cross-links and/or unreacted groups,  
 589 and which did not fully reach equilibrium after an aging time of  
 590 2 days (Figure S6).

The four IPNs also show an extended linear regime. As for  
 the single networks, as long as the strain sweep test is stopped  
 before reaching the amplitude at which the samples break, the  
 data measured from low to high to low strain amplitude show a  
 good reversibility (Figure 8). Again, a hysteresis appears at a  
 high strain. The reversible bonds are forced to break under  
 large oscillatory shear to allow the sample to follow the  
 deformation, but as soon as the deformation is reduced, the  
 reversible bonds are able to quickly re-form. This shows the  
 ability of the networks to self-heal after a large deformation.

Interestingly, the evolution of the critical strain value  $\gamma_c$   
 between the single networks and the IPNs depends on the  
 considered combination of networks. In particular, while the  
 stiffest IPN network, built from oxime and Fe<sup>2+</sup>-Tpy bonds,  
 has a similar  $\gamma_c$  value to the oxime single network, the IPN  
 network containing oxime and the most labile supramolecular  
 bond, Zn<sup>2+</sup>-Tpy, displays a longer linear regime, correspond-  
 ing to a larger  $\gamma_c$  value. Similarly, the linear regime of the IPN  
 network formed from the long-lifetime Fe<sup>2+</sup>-Tpy complexes  
 and the weak acylhydrazone is longer than the linear regime of  
 the single network formed only from the Fe<sup>2+</sup>-Tpy complexes.  
 Thus, one can conclude that using IPNs allows a significant  
 increase of storage modulus while conserving, or even  
 improving, the deformability of the materials.

## CONCLUSIONS

In this work, we investigated the viscoelastic properties of  
 interpenetrated network hydrogels based on two orthogonal  
 types of reversible bonds: dynamic covalent bonds (DCBs)  
 and metal-ligand bonds, with the aim of creating very stable—  
 yet reversible—networks thanks to the presence of the DCBs,  
 while the more tunable metal-ligand interactions can be used  
 to adjust the material properties. In particular, we have studied  
 how the rheological properties of both networks are combined  
 and modified when these networks are interpenetrated. Four

625 IPN hydrogels were thus obtained by combining either a very  
626 stable and pH-insensitive DCB (oxime) or a slightly less stable  
627 and pH-sensitive DCB (acylhydrazone), with either a long-  
628 lifetime supramolecular interaction ( $\text{Fe}^{2+}$ -Tpy) or a more  
629 dynamic one ( $\text{Zn}^{2+}$ -Tpy).

630 The results show that the obtained IPN hydrogels exhibit a  
631 higher modulus compared to the simple addition of the moduli  
632 of the single networks. We attributed this observation to the  
633 fact that part of the entanglements between the chains of the  
634 two networks are trapped between associated stickers and,  
635 therefore, act as additional physical interactions governed by  
636 the dynamics of the stickers. The study also revealed that the  
637 partial relaxation of the IPNs is induced by the relaxation of  
638 the supramolecular network and takes place through a sticky  
639 Rouse relaxation. We then studied how lowering the pH can be  
640 used as a stimulus to affect the dynamics of the IPNs. In  
641 particular, we showed that a low pH strongly influences the  
642 stability of the acylhydrazone DCB network. At low pH, the  
643 acylhydrazone subnetwork relaxes faster than the  $\text{Fe}^{2+}$ -Tpy  
644 supramolecular network, which corresponds to an inversion of  
645 the relaxation times of the two subnetworks compared to  
646 neutral pH. Finally, we demonstrated that building IPNs allows  
647 a significant increase of storage modulus while conserving, or  
648 even improving, the deformability of the materials. Combining  
649 DCB and metal–ligand bonds seems thus a promising  
650 approach toward highly tunable interpenetrated network  
651 hydrogels. Their properties under elongation should now be  
652 investigated to study the role played by the two networks on  
653 their extensibility.

## 654 ■ ASSOCIATED CONTENT

### 655 **SI** Supporting Information

656 The Supporting Information is available free of charge at  
657 <https://pubs.acs.org/doi/10.1021/acs.macromol.0c00494>.

658 Experimental section; synthetic routes of TPy-DEG-  
659  $\text{NH}_2$ , TPy-DEG-AM, P(DMA-co-ketone), and P(DMA-  
660 co-Tpy); preparations of individual dynamic Schiff base  
661 bonding networks, individual metal–terpyridine bond-  
662 ing networks, single networks in water from mixed  
663 copolymers of P(DMA-co-ketone) and P(DMA-co-Tpy),  
664 and IPN hydrogels;  $^1\text{H}$  NMR spectra of P(DMA-co-  
665 ketone), P(DMA-co-Tpy), dihydrazide, bishydroxyl-  
666 amine, acylhydrazone network, and oxime network;  
667 oscillatory frequency sweeps and strain sweeps; and pH  
668 dependence of the dynamic moduli (PDF)

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## 691 Notes

692 The authors declare no competing financial interest.

## 693 ■ ACKNOWLEDGMENTS

694 This project was partially funded by the French Community of  
695 Belgium through ARC project no. 16/21-076. H.Y. acknowl-  
696 edges the China Scholarship Council for the support of Ph.D.  
697 fellowship. E.v.R. is research associate of the FRS-FNRS.

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