#### **RESEARCH ARTICLE**



# Characterization of a clinically used charcoal suspension for in vivo EPR oximetry

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#### Abstract

**Objectives** Electron paramagnetic resonance (EPR) oximetry using particulate materials allows repeatable measurements of oxygen in tissues. However, the materials identified so far are not medical devices, thus precluding their immediate use in clinical studies. The aim of this study was to assess the magnetic properties of Carbo-Rep<sup>®</sup>, a charcoal suspension used as a liquid marker for preoperative tumor localization.

**Materials and methods** Calibration curves (EPR linewidth as a function of  $pO_2$ ) were built using 9-GHz EPR spectrometry. The feasibility of performing oxygen measurements was examined in vivo by using a low-frequency (1 GHz) EPR spectrometer and by inducing ischemia in the gastrocnemius muscle of mice or by submitting rats bearing tumors to different oxygen-breathing challenges.

**Results** Paramagnetic centers presenting a high oxygen sensitivity were identified in Carbo-Rep<sup>®</sup>. At 1 GHz, the EPR linewidth varied from 98 to 426  $\mu$ T in L-band in nitrogen and air, respectively. The sensor allowed repeated measurements of oxygen over 6 months in muscles of mice. Subtle variations of tumor oxygenation were monitored in rats when switching gas breathing from air to carbogen.

Discussion The magnetic properties of Carbo-Rep<sup>®</sup> are promising for its future use as oxygen sensor in clinical EPR oximetry.

Keywords  $EPR \cdot ESR \cdot Oximetry \cdot Charcoal \cdot Tumor hypoxia$ 

## Introduction

Oxygen is a critical factor in physiology, pathophysiology, and therapy. In many circumstances, the ability to measure oxygenation is critical to assess tissue function and disease. Several potentially useful methods are able to measure tissue oxygen level [1–3]. These methods are based on the accumulation of nitroimidazoles in hypoxic cells evidenced by immunohistochemistry [4] or positron emission tomography (PET) [5], fluorescence and phosphorescence quenching [6], electrochemical reaction [7], and magnetic resonance (MR) techniques. Oxygen-sensitive MRI techniques include  $T_2^*$ and  $T_1$  measurements [8–13], as well as fluorine relaxometry

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Bernard Gallez Bernard.Gallez@uclouvain.be [14, 15], as illustrative examples. Electron paramagnetic resonance (EPR) offers the possibility of providing quantitative pO<sub>2</sub> values using paramagnetic centers sensitive to the oxygen environment [16-20]. Among the potential EPR oxygen sensors, particulate materials offer several advantages: they are highly sensitive to variations of oxygen (changes <1 mmHg can be detected), and they are inert in tissues, leading to the possibility of repeat oxygen measurements from the same site over long periods (months to years) [16, 17, 19]. Several particulate materials have been identified for that purpose: lithium phthalocyanine [21] and substituted lithium naphthalocyanine [22], charcoals [23], and carbon blacks [24]. These particulate sensors were successfully used in preclinical studies to measure oxygen in brain [25], heart [26], skeletal muscle [27], liver [28], gastrointestinal tract [29], kidney [30], skin [31], ovarian grafts [32], pancreatic islet grafts [33], and wounds [34]. One of the largest successes of EPR oximetry has been the monitoring of variations in tumor oxygenation induced by pharmacological agents [35–41] or during the course of radiation therapy [42-45].

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The development of advanced whole-body low-frequency EPR systems [46] has opened up the possibility of translating this unique technology to measure tissue oxygenation in patients [47, 48]. When moving into the clinical arena, the most crucial issue is to ensure the biocompatibility of the oxygen sensors [49]. The seminal idea was to use India ink [50], which contains carbon-black particles, as this material has been used for several centuries for tattooing humans. However, as the paramagnetic properties largely varied from batch to batch, synthetic biocompatible India inks were developed using well-characterized carbon-black materials [24] and suspended in pharmaceutical-grade suspending agents [51]. Besides the use of inks, many efforts focused on the inclusion of paramagnetic sensors in thin oxygenpermeable biocompatible materials [52–58]. Still, researchers with an interest in applying EPR oximetry in patients are facing regulatory problems, namely, the need for production of experimental oxygen sensors according to good manufacturing practice (GMP) standards and the potential request for approval as an authorized medical device. These regulatory issues encouraged us to screen the EPR properties and oxygen sensitivity of carbon materials already approved as medical devices. From this screening, we identified Carbo-Rep<sup>®</sup> as a promising candidate for the application of EPR oximetry in patients. Carbo-Rep<sup>®</sup> is a sterile suspension of charcoal that is used in Europe for the accurate preoperative localization of mammographically detected lesions. This charcoal suspension is approved as a medical device class IIb. In this publication, we described the EPR characteristics of this charcoal with a focus on its sensitivity to oxygen. In addition, we performed in vivo experiments in mice and rats using low-frequency EPR to assess its ability to identify subtle variations of oxygenation in muscle and tumors and its long-term responsiveness as an oxygen sensor.

# **Materials and methods**

## Chemicals

Carbo-Rep<sup>®</sup> (40 mg charcoal/ml) was purchased from Sterylab (Milan, Italy). The suspension was shaken before sampling. All measurements were carried out on the suspension as received without any additional chemicals. The following batches were analyzed: nos. 0613-17 and 1152-17.

## **Particle size**

The particle size and the polydispersity index (PDI) were characterized by dynamic light scattering (DLS) using a Zetasizer Nano ZS (Malvern Instruments Ltd., Worcestershire, UK).

#### In vitro 9-GHz EPR spectrometry

EPR measurements were performed using a Bruker EMX-Plus spectrometer (Bruker, Rheinstetten, Germany) operating at X-band (9.4 GHz) and equipped with a PremiumX ultra-low-noise microwave bridge and a Super High Q (SHQ) high-sensitivity resonator. EPR settings were as follows: microwave power 1.262 mW; modulation frequency 100 kHz; modulation amplitude 0.02 mT; time constant 10.24 ms; conversion time 15 ms; data points 3000; sweep width 3 mT. Calibration curves of linewidth (LW) as a function of  $pO_2$  were done at 296 and 310 K. Approximately 50µl of charcoal suspension were placed in a gas-permeable Teflon tube (inner diameter 0.025 in.; outer diameter 0.029 in.; Zeus Industrial Products, Letterkenny, Ireland). The Teflon tube was inserted in a quartz tube open at both ends. The oxygen content was varied between 0 and 21% O<sub>2</sub> using an Aalborg gas mixer. The oxygen content in the mixed gas was measured using a Servomex MiniMP 5200 oxygen analyzer (precision 0.1% oxygen content). The gas flux in the EPR cavity was 270 l/h.

#### In vitro 1-GHz EPR spectrometry

The oxygen calibration curve at 310 K was also performed on a low-frequency EPR spectrometer (Clin-EPR LLC, Lyme, NH, USA) equipped with a loop-gap surface coil. Approximately 500 $\mu$ l of charcoal suspension was placed in a glass vial, which was placed in a water bath at 310 K. A gas with oxygen content varying between 0 and 21% O<sub>2</sub> was flushed for 75 min in the suspension through a needle. A second needle, inserted in the plug, was used to avoid hyperpressure in the vial. The oxygen content in the mixed gas was measured by a Servomex MiniMP 5200 oxygen analyzer. Needles were removed and vials placed on the loop-gap surface coil. EPR measurements were performed immediately.

#### In vivo 1-GHz EPR spectrometry

#### Anesthesia

Animals were anesthetized by inhalation of isoflurane mixed with air (21% oxygen) in a continuous flow (2 l/h) delivered by a nose cone. Induction of anesthesia was performed using 3% isoflurane which was then stabilized at 1.5% for a minimum of 15 min before any measurement. It was previously demonstrated that this anesthesia regimen did not disturb the hemodynamics in rodents [59]. A circulating water system was used for body-temperature regulation at 37 °C.

#### Muscle

Male C57BL/6 mice (Janvier, Le Genest-Saint-Isle, France) (n=5) were used for the studies in muscle; 75 µl of charcoal suspension was injected in both gastrocnemius muscles. The first EPR measurement was done 1 day after administration of the oxygen sensor. Measurements were repeated over 6 months. In vivo measurements were performed using a low-frequency EPR spectrometer (Clin-EPR LLC) equipped with a loop-gap surface coil. In two of five experimental animals, measurements were carried out on muscles before and after transient restriction of the blood supply (the base of the thigh was reversibly tied for 5 min with a thread to restrict flow through the femoral arteries). In total, ten muscles were measured at the basal state at each time point over 6 months and four muscles during transient ischemic periods.

#### Tumors

Seven-week-old male Fischer 344 rats (Charles River, Arbresle, France) (n=3) were subcutaneously injected with 5.10<sup>6</sup> 9L-glioma cells (kindly provided by Dr. Olivier Bockstael, Université Libre de Bruxelles, Belgium) in the thigh. Tumor implantation was performed under anesthesia with a mixed solution of ketamine and xylazine at doses of 80 and 10 mg/kg, respectively. Rats were included in the study when the tumor reached a diameter of 14-16 mm. Approximately 400µl of charcoal suspension was introduced within the tumor at a depth of 3-6 mm. EPR acquisitions were first carried out at 1 day after probe implantation. After recording the pO<sub>2</sub> value under normoxic condition, the input gas was switched from air to carbogen (5%  $CO_2$  in oxygen). The pO<sub>2</sub> value under hyperoxic condition was obtained after 30-min carbogen breathing. The experiment was repeated the following day (2 days after probe implantation) with the same animals.

# Results

The Carbo-Rep<sup>®</sup> preparation is a suspension of charcoal particles with a small diameter (mean 2.9  $\mu$ m, PDI=0.55), allowing easy sampling for injection. This charcoal suspension presents an EPR spectrum characteristic of a carbon-centered radical (Fig. 1) with a g-value of 2.00315. The microwave-power saturation curve is presented in Fig. 1. Interestingly, the EPR LW was highly sensitive to the oxygen environment, as shown in Fig. 1. The calibration curves (LW as a function of % oxygen) recorded in X-Band and L-Band are presented in Fig. 2. This calibration was



Fig. 1 Electron paramagnetic resonance (EPR) characteristics of the charcoal suspension present in Carbo-Rep<sup>®</sup>. Top: EPR spectra recorded at 9 GHz in air and in nitrogen. Bottom: microwave-power saturation curve

reproducible from vial to vial and from batch to batch (Fig. 2 top). We found that the calibration was slightly dependent on the temperature (Fig. 2 middle). In L band (Fig. 2 bottom), we observed a slightly different calibration compared to X band, particularly < 2% O<sub>2</sub>, where LW was lower for the same O<sub>2</sub> percentage. Low-frequency (1 GHz) EPR spectrometry was used to assess the performance of Carbo-Rep<sup>®</sup> as an oxygen sensor in vivo. Figure 3 presents a typical EPR spectrum recorded in vivo in the muscle after administration of 75µl of charcoal suspension. The LW varied considerably when the blood flow was temporarily interrupted in the muscle (Fig. 3). We repeated the measurements of the LW over a period of 6 months, which showed that Carbo-Rep<sup>®</sup> preserved its responsiveness to variations in oxygenation in vivo (Fig. 4). Mean pO<sub>2</sub> values are presented in Fig. 4. As expected, the administration of Carbo-Rep<sup>®</sup> induced no inflammatory response or damage in the muscle injected (Fig. 5). Carbo-Rep® was also administered in a glioma tumor model. The charcoal was distributed over the whole tumor, allowing measurement of the pO2 distributed in the whole tumor (Fig. 6). Baseline pO<sub>2</sub> values (while rats were breathing air) indicated that these tumors were highly



**Fig. 2** Calibration curves [linewidth (LW) as a function of percent  $O_2$ ] of charcoal suspension present in Carbo-Rep<sup>®</sup>. Top: oxygen calibrations carried out on three different flasks in X band. Closed circle: batch no. 0613-17 vial 1; Open circle: batch no. 0613-17 vial 2; Closed square: batch no. 1152-17 vial 1. Middle: effect of temperature on oxygen calibration in X band. Open circle: 296 K. Closed circle: 310 K. Bottom: oxygen calibration performed in L band (1 GHz). Results are expressed as mean  $\pm$  standard deviation (SD) (n=4)

hypoxic (Fig. 7). Individual tumor responses to a carbogenbreathing challenge are also presented. There was a large heterogeneity in response to carbogen breathing: the  $pO_2$ reached values >10 mmHg in three of six tumors. Overall, the increase in  $pO_2$  was significant.



**Fig.3** Typical electron paramagnetic resonance (EPR) spectra recorded in vivo using a 1-GHz EPR spectrometer in the gastrocnemius muscle of a mouse before and after transient restriction of the blood flow



**Fig. 4** Measurements of line width (LW) and pO<sub>2</sub> estimates recorded in vivo in the muscle of mice after administration of Carbo-Rep<sup>®</sup>. Top: electron paramagnetic resonance (EPR) LW measured over time in normal muscles (n=10, open circle) and hypoxic muscles (n=4, closed square). Bottom: mean pO<sub>2</sub> values±standard error of mean (SEM) measured in muscles and hypoxic muscles. \*\*\*\*P<0.0001



Fig. 5 Histological section in a muscle injected with Carbo-Rep<sup>®</sup> ( $\mathbf{a}$ ) and magnification of area close to sensor location ( $\mathbf{b}$ ). Minimal inflammation, if any, was observed around the charcoal material



Fig. 6 Distribution of the charcoal inside a tumor

## Discussion

While tissue oxygenation is critical in the management of many pathologies, current clinical practice often uses indirect markers of tissue hemodynamics. However, there are several circumstances in which the knowledge of real  $pO_2$ values could potentially impact the clinical decision. The most obvious field is radiation therapy, as the response to irradiation is dramatically dependent on pO<sub>2</sub> values in the range of 0–10 mmHg [60–63]. Eppendorf<sup>®</sup> pO<sub>2</sub> histograph has been used over the past two decades to definitely establish the relevance of pO<sub>2</sub> measurements in radiation therapy [7], but its invasive nature led to its withdrawal from clinical practice. Among methods that are reporting actual pO2 values, EPR offers the unique advantage of repeatable measurements from the same site over time after a single administration of an oxygen sensor [64]. Pioneering clinical EPR studies have used inks made of carbon black or charcoal particles [47, 48, 50, 64-66]. To pursue and extend the clinical EPR oximetry studies, there is a crucial



**Fig. 7**  $pO_2$  measurements (n=6) recorded in 9-L gliomas (in rats) after administration of Carbo-Rep<sup>®</sup>. Top: individual responses when switching from air to carbogen breathing. Bottom: mean  $pO_2$  values±standard error of mean (SEM) measured before and after 30 min carbogen breathing. \*P=0.0353

need for the use of paramagnetic oxygen-sensitive probes that are recognized as medical devices. From our screening on carbon-based materials used in preoperative marking, our attention was drawn to Carbo-Rep<sup>®</sup>. We found that this material presents a single-line EPR spectrum, with an LW highly sensitive to the oxygen environment (Fig. 1). The calibration curve (LW as a function of pO<sub>2</sub>, Fig. 2) is comparable with other carbon-based oxygen-sensitive materials previously described [23, 24, 67, 68]. Interestingly, this charcoal formulation offers the maximal sensitivity in the range of physiological tissue oxygenation values (0-5% oxygen, or 0-38 mmHg) (Fig. 2). In addition, the accuracy of measurement was high, with an error estimated at ~0.5 mmHg at 1% oxygen. We also observed that variation in temperature may slightly affect the calibration (Fig. 2). As a consequence, for an accurate estimate of the  $pO_2$ , it is important to keep tissue temperature constant during measurements, especially when sedation or anesthesia is necessary. The injection of a small amount (75µl) of Carbo-Rep<sup>®</sup> suspension allowed recording an EPR signal using a Clin-EPR system (1-GHz EPR spectrometer) that could be further analyzed for LW estimation (Fig. 3). In muscles, the pO<sub>2</sub> measurements using EPR and Carbo-Rep<sup>®</sup> as the oxygen sensor were well within the range of physiological values found in other studies [27, 54, 55, 58]. As responsiveness stability is a critical issue when evaluating the performance of an oxygen sensor [53-55, 58], in vivo EPR measurements were repeated over a period of 6 months. Both baseline values and response to blood-flow restriction (Fig. 4) demonstrated Carbo-Rep® application allows for long-term oximetry. This feature is particularly interesting considering that clinical application of an EPR oxygen sensor has the potential for longterm monitoring of hypoxic status and oxygen changes in peripheral vascular diseases, wound healing [69, 70], and during the time course of radiation therapy [48, 71, 72]. To assess its potential application in the latter scenario, we administered Carbo-Rep® in a tumor model and evaluated the response to carbogen breathing, a treatment often used in an attempt to increase tumor oxygenation. We found that this charcoal preparation was capable of monitoring subtle changes in tumor oxygenation.

# Conclusion

We identified a registered medical device that fulfills the requirements for oxygen measurements using EPR oximetry. This material, which is used clinically for preoperative localization of breast cancer, possesses EPR properties favorable for use as an oxygen sensor in future clinical EPR studies.

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Author contributions CMD, LBAT, PD: data acquisition, analysis, and interpretation; manuscript drafting; critical revision. BG: study

conception and design; data analysis and interpretation; manuscript drafting; critical revision.

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### **Compliance with ethical standards**

**Conflict of interest** The authors declare that they have no conflict of interest.

**Statement of human rights** This article does not contain any studies with human participants performed by any of the authors

Statement on the welfare of animals All applicable international, national, and/or institutional guidelines for the care and use of animals were followed. All procedures performed in studies involving animals were in accordance with the ethical standards of the institution or practice at which the studies were conducted (authorization 2014/UCL/MD/026).

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